

## DESIGN AND IN VITRO AND IN VIVO EVALUATION OF FLOATING MICROSPHERES OF METFORMIN HYDROCHLORIDE FOR ORAL CONTROLLED RELEASE

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### **ABSTRACT**

The floating microspheres have been utilized to obtain prolonged and uniform release in stomach for development of a once daily formulation. The major advantage of preparation technique includes short processing time, lack of exposure of ingredients to high temperature, and high encapsulation efficiencies. In the present study, preparation of metformin hydrochloride floating microspheres, evaluation of Floating Drug Delivery System in vitro release, optimization of floatation and drug release pattern to match target release profile was investigated. Floating microspheres were prepared by Single Emulsion Solvent Evaporation Method using Eudragit RS100 controlling polymer and 250 mg of metformin hydrochloride per batch and its in vitro release performance was evaluated by the usual pharmacopoeial and other tests such as yield(%), particle size analysis, floating ability, drug entrapment efficiency, surface topography and release studies. The result showed that mixing ratio of

components in organic phase affected the size distribution (206.3-469.8  $\mu\text{m}$ ), drug entrapment efficiency (58.27-40.06(% wt/wt), % yield (78.27-75.44% wt/wt), floating ability (82.67-60.84 %) and drug release of floating microspheres (53.06-74.84% after 12 hrs), floating duration (8-12 hrs) and the best results were obtained at the ratio of drug: polymer, stirring speed, droplet stabilizer(1:5, 700rpm, 10% wt/wt). In case of floating microspheres of metformin hydrochloride, the reduction in glucose levels was slower and found to be  $106.00 \pm 0.54 \text{mg/dl}$  reached 8 hours after oral administration. The sustain hypoglycemic effect

observed over longer periods of time in the case of floating microspheres is due to the controlled release and absorption of metformin hydrochloride over longer period of time.

**KEYWORDS:** floating microspheres, metformin hydrochloride, controlled release.

## INTRODUCTION

Floating drug delivery systems has been a topic of interest in the design of drug delivery systems to prolong the residence time of the dosage form at the site of application or absorption and to facilitate intimate contact of the dosage form with the underlying absorption surface to improve and enhanced bioavailability of drugs.<sup>[1,2]</sup> Several studies reported Floating drug delivery systems in the form of tablets, capsules, beads, and granules for oral routes; however, very few reports on floating microspheres are available. The objective of this study is to develop, characterize, and evaluate floating microspheres of metformin hydrochloride employing low density base polymers for prolonged gastrointestinal absorption. Metformin hydrochloride, an effective antidiabetic that requires controlled release owing to its short biological half-life of  $5.4 \pm 0.6$  hours, was used as the core in microencapsulation.<sup>[3,4]</sup> The floating microspheres were evaluated by in vitro and in vivo methods for controlled release.

## MATERIALS AND METHODS

### Materials

Metformin hydrochloride was a gift sample from M/s Cadila health care (Ahmedabad India). Eudragit RS 100 was a gift sample from M/s Cadila health care (Ahmedabad India). Magnesium stearate were procured from commercial sources. All other reagents used were of analytical grade.

### Methods

#### *Single Emulsion Solvent Evaporation Method*

Microspheres containing metformin hydrochloride were prepared by single emulsion solvent evaporation method (Eudragit RS 100 1250mg) and active substance metformin hydrochloride (250mg) were dispersed in ethanol (50ml) and mixed through with a magnetic stirrer to form a clear solution.

In this method the drug – metformin hydrochloride and polymer- Eudragit RS100 into 1:5 ratios were dispersed in 50ml ethanol. Magnesium stearate (10%wt/wt) was dispersed in the

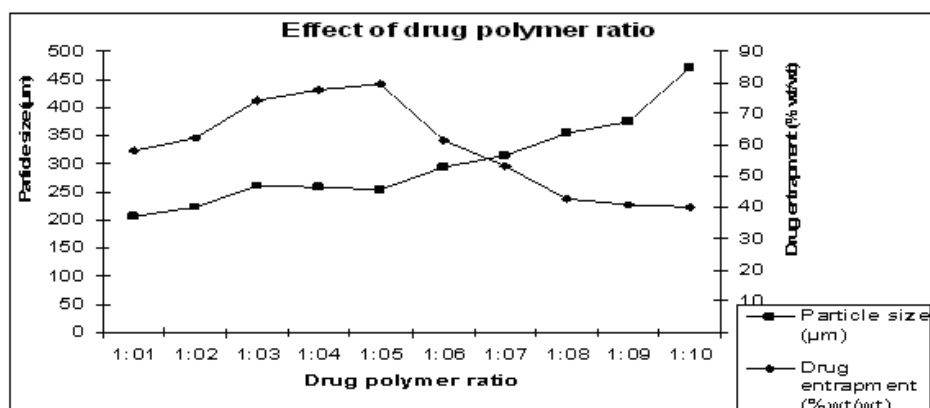
drug and polymer solution which acted as a droplet stabilizer. The dispersion was added to 250ml of light liquid paraffin containing 30ml n-hexane with continuous mechanical stirring at 700rpm. Stirring was continued for two hours, until ethanol evaporated completely. The microspheres formed were collected by filtration in vacuum, washed repeatedly with petroleum ether each and dried at  $30\pm 2^{\circ}\text{C}$  for 24 hours. The microspheres prepared along with their drug: polymer are listed in Table 1.<sup>[5, 6, 8]</sup>

#### Optimization of drug and polymer ratio

Various batches F1, F2, F3, F4, F5, F6, F7, F8, F9 and F10 with different drug: polymer ratio i.e. 1:1, 1:2, 1:3, 1:4, 1:5, 1:6, 1:7, 1:8, 1:9, and 1:10 were prepared by single emulsion solvent evaporation method. Keeping stirring speed 700rpm, droplet stabilizer magnesium stearate (150mg) and solidifying agent n-hexane.

**Table 1: Optimization of drug and polymer ratio.**

Batch	Drug: Polymer	Mean $\pm$ S. D., n=20		Mean $\pm$ S. D., n=3			
		Average Diameter ( $\mu\text{m}$ )	Floating Duration (Hrs)	Floating Ability (%)	Yield (%wt/wt)	DEE (%wt/wt)	Drug Loading (%wt/wt)
F1	1:01	206.3( $\pm 2.497$ )	11	82.673( $\pm 0.577$ )	78.27( $\pm 0.015$ )	58.27 ( $\pm 0.020$ )	25.32( $\pm 0.010$ )
F2	1:02	223.7( $\pm 2.946$ )	11	84.83 ( $\pm 0.763$ )	79.02 ( $\pm 0.009$ )	62.36 ( $\pm 0.025$ )	18.88 ( $\pm 0.015$ )
F3	1:03	259.8( $\pm 4.315$ )	12	86.01( $\pm 0.215$ )	79.05 ( $\pm 0.040$ )	74.22 ( $\pm 0.015$ )	17.24 ( $\pm 0.010$ )
F4	1:04	259.1( $\pm 4.818$ )	12	89.60 ( $\pm 0.360$ )	81.18 ( $\pm 0.042$ )	77.51 ( $\pm 0.015$ )	14.60( $\pm 0.020$ )
F5	1:05	255.1( $\pm 2.726$ )	12	95.47 ( $\pm 0.416$ )	82.56 ( $\pm 0.035$ )	79.38 ( $\pm 0.015$ )	12.61( $\pm 0.010$ )
F6	1:06	293.5( $\pm 2.838$ )	10	79.78 ( $\pm 0.503$ )	80.99 ( $\pm 0.100$ )	61.32 ( $\pm 0.010$ )	8.38( $\pm 0.010$ )
F7	1:07	314.7( $\pm 7.040$ )	10	73.72 ( $\pm 0.249$ )	79.23 ( $\pm 0.035$ )	53.32 ( $\pm 0.015$ )	6.42( $\pm 0.005$ )
F8	1:08	354.5( $\pm 5.949$ )	9	68.47 ( $\pm 0.551$ )	77.82 ( $\pm 0.020$ )	42.73( $\pm 0.026$ )	4.58( $\pm 0.017$ )
F9	1:09	375.1( $\pm 8.252$ )	8	64.90 ( $\pm 0.360$ )	74.55 ( $\pm 0.026$ )	41.04 ( $\pm 0.051$ )	3.97( $\pm 0.005$ )
F10	1:10	469.8( $\pm 5.978$ )	8	60.84 ( $\pm 0.764$ )	75.44 ( $\pm 0.210$ )	40.06( $\pm 0.065$ )	3.53( $\pm 0.005$ )



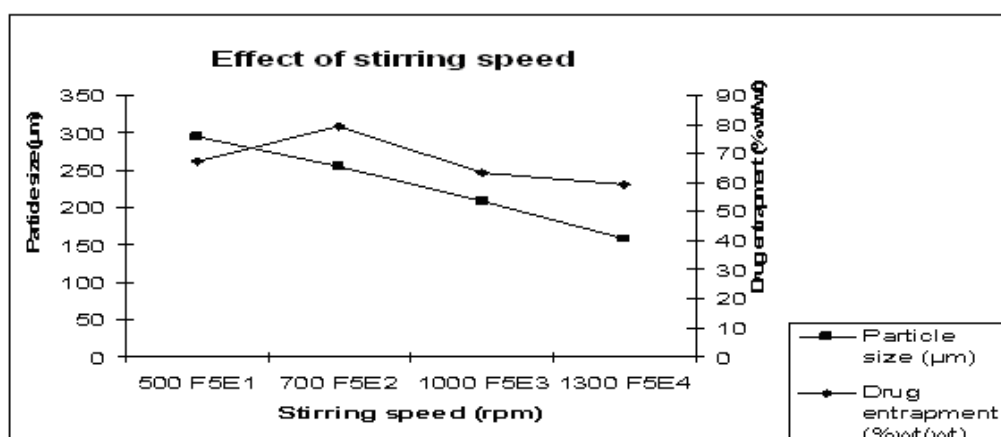
**Figure 1: Effect of Drug-polymer ratio on average particle size and percent drug entrapment.**

#### Optimization of Stirring Speed

Floating microspheres were prepared by single emulsion solvent evaporation method with optimized ratio of drug and polymer ( 1:5 ) keeping the quantity of droplet stabilize and hardening agent constant, utilizing four different speeds i.e. 500, 700, 1000 and 1300 rpm.

**Table 2: Optimization of Stirring Speed.**

Batch	RPM	Mean $\pm$ S. D., n=20	Mean $\pm$ S. D., n=3				
		Average Diameter ( $\mu\text{m}$ )	Floating Duration (Hrs)	Floating Ability (%)	Yield (%wt/wt)	DEE (%wt/wt)	Drug Loading (%wt/wt)
F5E1	500	294.5( $\pm$ 2.890)	11	81.67( $\pm$ 0.432)	77.27( $\pm$ 0.028)	67.51( $\pm$ 0.020)	10.71( $\pm$ 0.015)
F5E2	700	255.1( $\pm$ 2.726)	12	95.47 ( $\pm$ 0.416)	82.56 ( $\pm$ 0.035)	79.38 ( $\pm$ 0.015)	12.61( $\pm$ 0.010)
F5E3	1000	208.3( $\pm$ 2.577)	10	80.56( $\pm$ 0.341)	75.27( $\pm$ 0.020)	63.32 ( $\pm$ 0.027)	10.02( $\pm$ 0.013)
F5E4	1300	159.0( $\pm$ 1.630)	10	78.23( $\pm$ 0.540)	73.27( $\pm$ 0.040)	59.30 ( $\pm$ 0.022)	9.41( $\pm$ 0.011)



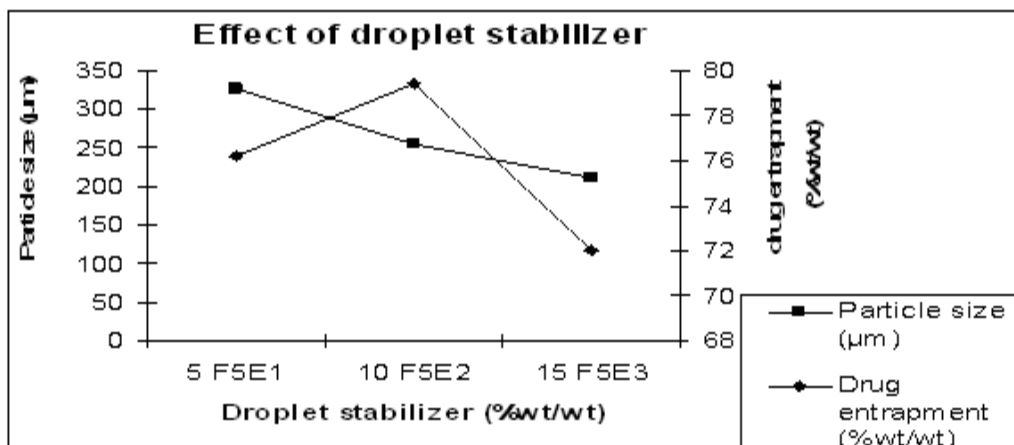
**Figure 2: Effect of stirring speed on average particle size and percent drug entrapment.**

#### Optimization of Quantity of Droplet Stabilizer

Floating microspheres were prepared by keeping drug polymer ratio (1:5) and stirring speed (700) constant taking 5, 10 and 15% wt/wt of magnesium stearate.

**Table 3: Optimization of quantity of droplet stabilizer.**

Batch	Droplet stabilizer (%wt/wt)	Mean $\pm$ S. D., n=20	Mean $\pm$ S. D., n=3				
		Average Diameter ( $\mu\text{m}$ )	Floating Duration (Hrs)	Floating Ability (%)	Yield (%wt/wt)	DEE (%wt/wt)	Drug Loading (%wt/wt)
F5E1	5	325.5( $\pm$ 7.255)	10	80.59( $\pm$ 0.344)	78.20( $\pm$ 0.039)	76.21( $\pm$ 0.014)	12.05( $\pm$ 0.012)
F5E2	10	255.1( $\pm$ 2.726)	12	95.47 ( $\pm$ 0.416)	82.56 ( $\pm$ 0.035)	79.38 ( $\pm$ 0.015)	12.61( $\pm$ 0.010)
F5E3	15	210.0( $\pm$ 2.595)	10	78.25( $\pm$ 0.544)	80.20( $\pm$ 0.042)	72.05( $\pm$ 0.014)	11.43( $\pm$ 0.011)



**Figure 3: Effect of Droplet stabilizer on average particle size and percent drug entrapment.**

### *Characterization and Evaluation of Floating Microspheres*

#### *Scanning electron microscopy*

The microspheres were observed under a scanning electron microscope. They were mounted directly onto the SEM sample stub using double-sided sticking tape and coated with gold film under reduced pressure (0.001mm of Hg).



**Figure 4: SEM photograph of metformin hydrochloride floating microspheres**

#### *Drug loading, Drug Entrapment Efficiency*

A quantity of microspheres containing equivalent to 50mg of metformin hydrochloride was taken for evaluation. The amount of drug entrapped was estimated by crushing the microspheres and extracting with aliquots 100ml of 0.1 N HCl repeatedly. The extract was transferred to a 100 ml volumetric flask and the volume was made up using 0.1N HCl. The solution was filtered and the absorbance was measured after suitable dilution

spectrophotometrically at 232nm against appropriate blank.<sup>[8]</sup> The amount of drug entrapped in the microspheres was calculated using the following formula.

Drug Entrapment Efficiency = (Amount of drug actually present / Theoretical drug load ) X 100.

Drug loaded on to the microspheres was estimated using the following formula.

Drug loading = (Amount of drug actually present/ total weight of microspheres) X 100

#### *In-Vitro Evaluation of Floating Ability*

The in vitro floating ability studies were carried out using Dissolution apparatus [USP XXIII apparatus no. 2 (paddle)].

In vitro floating ability of microspheres was studied simulated gastric fluid containing 1% Tween 80 as a dispersing medium. Microspheres were spread of over the surface of 900 ml of dispersion medium at  $37\pm 0.5^{\circ}\text{C}$  and agitated by a paddle rotating at 100rpm. Each fraction of microspheres floating on the surface and those settled down were collected at a predetermined time point. The collected samples were weighted after drying.

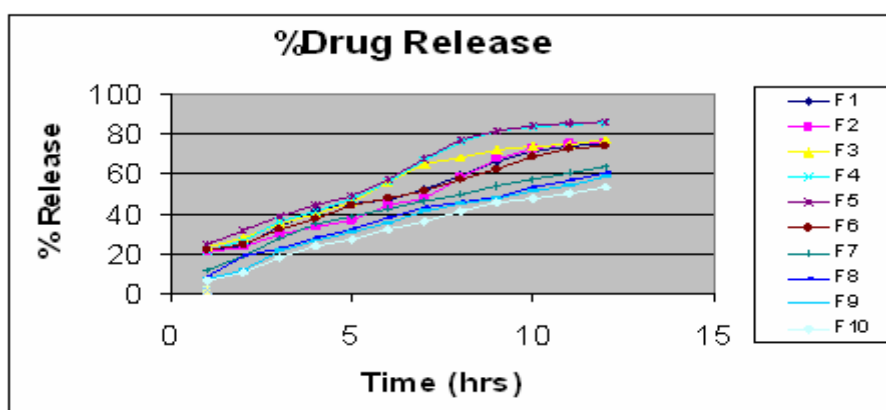
% floating microspheres = (Weight of floating microspheres / initial weight of floating microspheres) X 100

#### *In-Vitro Drug Release Study*

The in vitro drug release studies were carried out by paddle method using Dissolution apparatus [USP XXIII apparatus no. 2 (paddle)]. A quantity of microspheres equivalent to 100 mg of the drug was used. The 900ml of 0.1N HCl was used as dissolution fluid. The paddle was rotated at a speed of 100 rpm and the whole system was thermally controlled at  $37\pm 1^{\circ}\text{C}$ . Five ml of the aliquots were withdraw at predetermined time intervals and filtered through whatmann filter paper. The samples were suitable diluted with 0.1N HCl and the solutions were analyzed for the drug content spectrophotometrically at 232nm against reagent blank. The dissolution medium was replaced with same volume of 0.1N HCl to maintain sink condition.<sup>[8,9]</sup> From this percentage drug release is calculated and plotted against function of time study the pattern of drug release. The drug release experiments were conducted in triplicate (n=3).

**Table 4: Cumulative % release of metformin hydrochloride from floating microspheres in 0.1N HCl.**

Time(h)	Cumulative % drug release									
	F1	F2	F3	F4	F5	F6	F7	F8	F9	F10
1	21.45	20.79	22.76	21.45	24.33	21.58	11.74	8.46	7.28	6.1
2	23.94	23.15	27.33	26.43	31.15	24.46	18.3	18.82	11.47	10.03
3	33.12	29.58	34.43	35.75	38.63	32.33	27.87	22.5	21.31	18.03
4	41.91	33.12	39.68	40.99	44.14	37.19	34.3	27.48	26.04	23.41
5	44.67	36.27	45.59	47.55	49	44.54	38.5	31.94	30.63	27.09
6	46.77	44.01	55.56	55.95	56.74	47.55	42.31	37.84	35.35	32.2
7	51.87	47.55	64.74	66.97	67.5	51.1	46.37	42.83	40.86	36.14
8	59.23	57.39	68.2	75.63	76.68	57.26	49.39	45.72	45.06	40.73
9	66.31	67.5	71.96	81.4	81.66	62.12	53.59	47.82	47.29	45.32
10	70.91	72.48	73.96	83.5	84.29	68.81	57	53.06	51.1	47.55
11	73.79	74.71	74.45	84.42	85.34	72.74	60.54	56.34	53.59	49.91
12	74.84	75.37	76.68	85.21	85.6	73.79	63.69	60.41	58.31	53.06



**Figure 5: In-vitro release profile of floating microspheres of metformin hydrochloride in 0.1N HCl.**

#### *Kinetic modeling of drug release*

The dissolution profile of all the batches was fitted to zero order, first order, Higuchi, Hixon-crowell, Korsmeyer and Peppas to ascertain the kinetic modeling of drug release and the model with the highest correlation coefficient was considered to be the best model.<sup>[12,13,14]</sup>

#### *Stability study*

The floating microspheres of optimized formulation (F5) were put on short term stability study at 4°C, 40°C/75%RH and room temperature condition for the periods of three months. The floating microspheres were evaluated for residual drug content at after a period of 10, 20, 30, 60, and 90 day.<sup>[15]</sup>

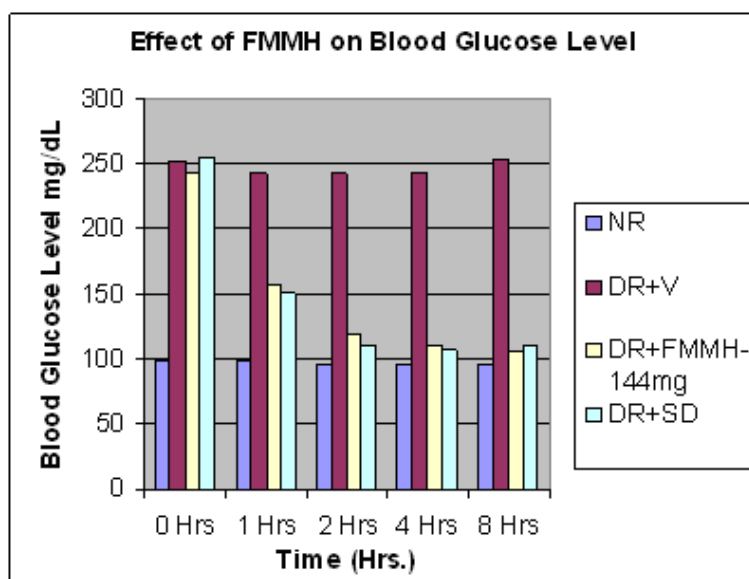
*In Vivo Evaluation*

The *in vivo* activity was required for controlled released action of floating microspheres over on conventional dosage form. The *in vivo* activity has been approved by Institutional Ethical Committee.

The animals used for experiment were adult male Albino rats (Wistar strain 150- 250g). Total of 24 rats were taken, 6 rats in each group, and were fasted 16 hours before the day of experiment with free access to water. Diabetes was induced in all rats by intraperitoneal injection of alloxan monohydrate. The dose of alloxan monohydrate was 125mg/kg body weight.<sup>[1, 3]</sup> The vehicle used for preparation of alloxan monohydrate was normal saline [0.9% w/v].

A blunt end cannula fitted with plastic syringe was used to administer orally the optimized formulation (floating microspheres of metformin hydrochloride), and standard drug (metformin hydrochloride). Animals of all the groups were treated with an oral D-glucose load of 2gm/kg by means of cannula. Group I was a normal group and group II was diabetic control group. Group III, IV were treated orally with floating microspheres of metformin hydrochloride at doses level of 144mg and standard drug (Metformin hydrochloride) 300mg/kg b.w. solution.

Blood samples were withdrawn from the tail of each rat using sharp sterile blade under light ether anesthesia after 0min, 1hrs, 2hrs, 4hrs and 8 hours and determined blood glucose concentration glucometer (Accu- Check).<sup>[16, 17]</sup>



**Figure 6: Effect of FMMH on blood glucose level**



### *Statistical analysis*

Analysis of variance (ANOVA) was performed to find out significant difference among the formulations having optimum floating and drug release using Prism software. ANOVA was applied on % cumulative drug release of metformin hydrochloride followed by Newman-Keuls Multiple comparison test.

## **RESULTS AND DISCUSSION**

The long term therapy of metformin hydrochloride is required for proper management of type-2 diabetes mellitus. Hence controlled drug delivery is demanded. Therefore, it was decided to formulate a therapeutic system bearing metformin hydrochloride, which delivers the drug through the oral route for prolonged period of time, decrease the dose related side effects and improve patient compliance.

The floating microspheres were prepared by single emulsion solvent evaporation technique by dissolving Eudragit RS 100 and metformin hydrochloride in ethanol under magnetic stirring. Magnesium stearate was selected as the droplet stabilizer. The process parameters which were optimized included drug: polymer ratio, stirring speed (rpm) and quantity of droplet stabilizer.

The mean diameter of floating microspheres of metformin hydrochloride was found to increase from 206.30 $\mu\text{m}$  to 469.80 $\mu\text{m}$  with increase in drug to polymer ratio from 1:1 to 1:10 (**Table 1, Figure 1**). This increase in particle size can be attributed to an increase in viscosity with increasing polymer concentration, which resulted in larger emulsion droplets and finally larger microspheres size.

The mean diameters of floating microspheres prepared using various agitation speeds (i.e. 500, 700, 1000 and 1300rpm) were 294.50, 225.10, 208.30 and 159.0 $\mu\text{m}$  respectively. It was found that particle size decreased with increase in speed of agitation. It was found that at 700rpm stable microspheres formulation was achieved at 700rpm with average particle size, maximum drug entrapment and maximum floating ability of 255.1 $\mu\text{m}$ , 79.38 % wt/wt and 95.47 % respectively. (**Table 2, Figure 2, Figure 4**).

The mean particle diameter of microspheres prepared using various quantity of droplet stabilizer (i.e. 5, 10 and 15% wt/wt) were 325.5, 255.1 and 210 $\mu\text{m}$  respectively. The mean particle size of floating microspheres was found to increase with decreasing amount of

magnesium stearate. As the droplet stabilizer amount increased, the shape of microspheres became irregular and the size of the microspheres was reduced from 325.5  $\mu\text{m}$  to 210  $\mu\text{m}$ . The size of microspheres was found to increase because low magnesium stearate content failed to prevent droplet coalescence in the oil medium. On the other hand the mean particle size decreased on increasing the amount of magnesium stearate (15% wt/wt). This was a consequence of stabilization of the oil droplets with magnesium stearate. Spherical, discrete microspheres were formed when magnesium stearate content was maintained at (10 % wt/wt). (**Table 3, Figure 3.**) Percent drug entrapment and loading were found to be 79.38 % wt/wt and 12.61 % wt/wt respectively.

In vitro drug release study for all the batches was carried out using USP type II apparatus using 0.1N HCl as dissolution medium, at 100rpm and  $37\pm 1^\circ\text{C}$ . All the batches showed an initial burst release (21.40-6.10)% in 1 hour which is attributed to surface associated drug, followed by a slower release phase as entrapped drug slowly diffuses out into the release medium. After 12 hrs 74.84-56.06% of drug was released for formulations F1 to F10. (**Table 4, Figure 5.**)

The optimized batch F5 showed an initial burst release (24.33%) in 1 hour attributed to surface associated drug, followed by a slower release phase as entrapped drug slowly diffuses out into the release medium, 85.6% drug was released after 12 hours. There was a sustained release of drug at a constant rate. The release of the drug at controlled rate from microparticles was due to the formation of pores. Kinetic models further support the above statements. The  $n$  value and  $r^2$  value of the optimized batch was found to be 0.5641 and 0.9741 respectively, which shows that the formulation released the drug by the process of diffusion.

The  $t_{10\%}$  obtained in case of formulation stored at  $4\pm 1^\circ\text{C}$  and  $40\pm 1^\circ\text{C}$  were found lower in comparison with the formulation stored at room temperature which indicated that the formulation tend to degrade faster at lower and higher temperatures. The results of stability studies suggest that for adequate shelf life of floating microspheres formulation the ideal storage temperature is room temperature.

In case of floating microspheres of metformin hydrochloride, the reduction in glucose levels was slower and found to be  $106.00\pm 0.54\text{mg/dl}$  reached 8 hours after oral administration. The sustain hypoglycemic effect observed over longer periods of time in the case of floating

microspheres was due to the controlled release and absorption of metformin hydrochloride over longer period of time. (**Figure 6**)

## CONCLUSION

Thus, spherical microspheres consisting of Eudragit RS100 containing metformin hydrochloride could be prepared by single solvent evaporation method. The microspheres exhibited good floating properties in an in vitro test. Metformin hydrochloride release from these floating microspheres slow and extended over longer periods of time. Drug release was diffusion controlled followed zero, Korsmeyer-Peppas, order kinetics after a long period of 12 hrs. in the in vivo evaluation Eudragit RS 100 floating microspheres could sustained the hypoglycemic effect of metformin hydrochloride over a 8 hrs period. These floating microspheres are thus, suitable for controlled release of metformin hydrochloride.

Results of present study provided an insight into the significance of floating microspheres as an oral delivery device for antidiabetic drug metformin hydrochloride. The investigated system has potential and is capable of maintaining constant drug concentration over prolonged period due to its controlled action. This can be expected to reduce the frequency of administration seen with repeated administration of conventional metformin hydrochloride loaded dosage forms, which ultimately improves the patient compliance.

It is concluded that a controlled release floating microspheres metformin hydrochloride formulation with satisfactory in vitro release characteristics and in vivo antidiabetic effect was successfully prepared.

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